

Toward the development of an *in silico* human model for indoor environmental design

Some arguments for developing *in silico* model for fluid-initiated environmental design research in an enclosed space

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Toward the development of *in silico* models for inhalation exposure analysis



Minimization of *in vivo/in vitro* experiments, and Maximization of *in silico* model application

Some arguments for developing *in silico* Laboratory Animal models for Inhalation Exposure Analysis



Upper Airway models for Surrogate Animals

Rat



Compact, genetic and environmental factors are completely controlled. Average life expectancy is around 1200 days, airway reactivity (high)



Rat (Sprague-Dawley)

Dog



Relatively small, genetic difference of individuals (small), fertility



Dog (Beagle)

Monkey



Temporomandibular joint, respiratory shape similar to human

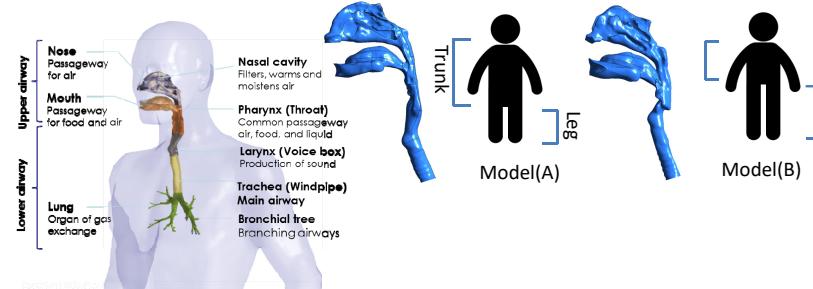


Monkey (Macaca fascicularis)

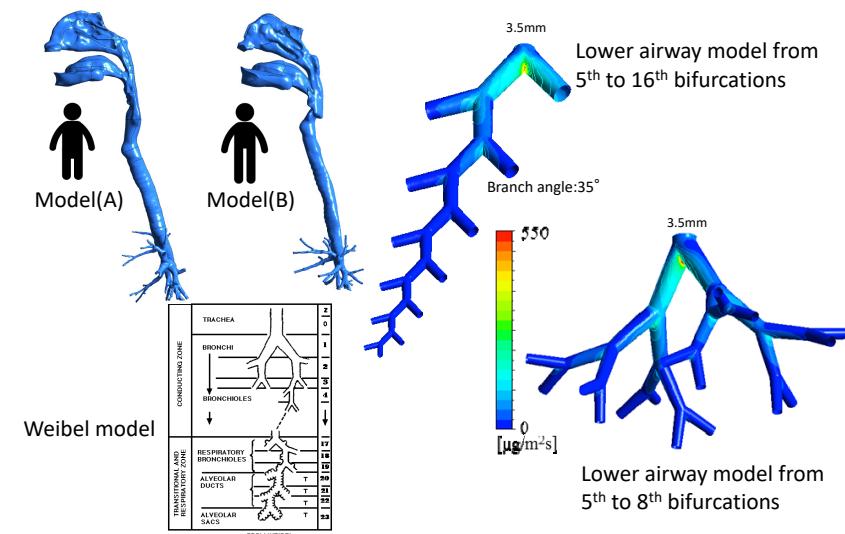
(Mitsumune, K. et al., 2016)

Upper Airway models for Humans

	Model (A) Japanese	Model (B) European
Body Height	1.7m	1.7m
BMI	21	21
Size (Height of Virtual Airway)	0.34568m	0.27381m
Inner Surface area (A)	0.057967m ²	0.044637m ²
Volume (V)	1.7336×10^{-4} m ³	1.2862×10^{-4} m ³
V/A	2.9908×10^{-3} m	2.8814×10^{-3} m



Upper and Lower Airway models for Humans



Detail Geometry Data for *in silico* models

	Rat	Dog	Monkey	Model (A) Japanese	Model (B) European
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Total inner surface area	3.62×10^{-6} [m ²]	1.29×10^{-4} [m ²]	2.81×10^{-5} [m ²]	2.19×10^{-4} [m ²]	2.14×10^{-4} [m ²]
Total length	55.10 [mm]	1.45×10^{-1} [m]	1.05×10^{-1} [m]	2.39×10^{-1} [m]	1.95×10^{-1} [m]
Maxi. height	18.30 [mm]	7.16×10^{-2} [m]	4.32×10^{-2} [m]	1.46×10^{-1} [m]	1.34×10^{-1} [m]
Maxi. width	16.00 [mm]	4.97×10^{-2} [m]	2.8110^{-2} [m]	6.21×10^{-2} [m]	6.21×10^{-2} [m]
Area of naris/ Eq. diameter	3.72×10^{-7} [m ²] / 6.89×10^{-4} [m]	6.00×10^{-5} [m ²] / 8.74×10^{-3} [m]	5.48×10^{-6} [m ²] / 2.64×10^{-3} [m]	8.00×10^{-5} [m ²] / 1.00×10^{-2} [m]	8.00×10^{-5} [m ²] / 1.00×10^{-2} [m]
Area of naris/ Eq. diameter	3.08×10^{-7} / 6.27×10^{-4} [m]	5.28×10^{-5} / 8.20×10^{-3} [m]	5.46×10^{-6} [m ²] / 2.64×10^{-3} [m]	8.00×10^{-5} [m ²] / 1.00×10^{-2} [m]	8.00×10^{-5} [m ²] / 1.00×10^{-2} [m]

1.4% 34.7% 8.8% of Human model (A)

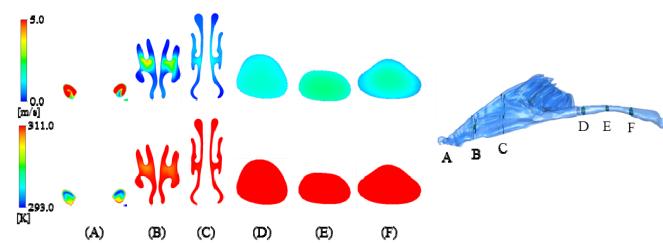
Numerical Boundary Conditions

	Rat	Dog	Monkey	Model (A) Japanese	Model (B) European
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Model geometry					
Mesh (Unstructured, Tetra mesh)	5.34M	6.49M	7.03M	7.25M	3.81M
Outflow boundary [L/min]	0.275	3.5	2.0	7.5	7.5
Re number	186.1	396.9	485.3	652.9	660.5
Wall treatment	311K Velocity : no slip	311K Velocity : no slip	310.8K Velocity : no slip	309.8K Velocity : no slip	309.8K Velocity : no slip
Inflow boundary					
Turb. model	Nasal opening : $U_{in} = k_{in} = \epsilon_{in}$ =Gradient zero				
	Low Re Type k-ε model (Abe- Kondoh- Nagano Model, 3D Cal.)				

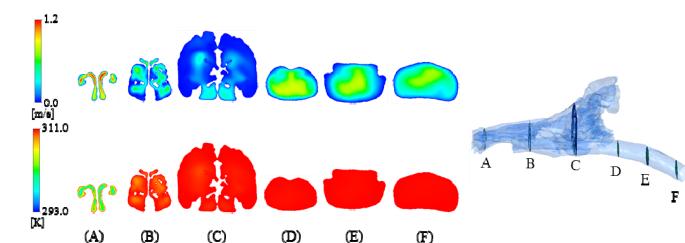
Rat



(1) $Q_{in}=0.275 \text{ L/min}$ (2) $Q_{in}=0.55 \text{ L/min}$ (3) $Q_{in}=1.1 \text{ L/min}$

Convective heat transfer flux distributions on the upper airway surfaces of the rat

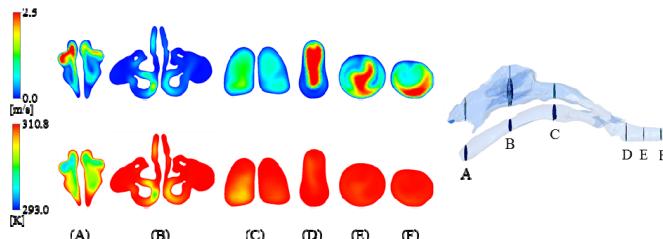
Dog



(1) $Q_{in}=3.5 \text{ L/min}$ (2) $Q_{in}=7.0 \text{ L/min}$ (3) $Q_{in}=10.5 \text{ L/min}$

Convective heat transfer flux distributions on the upper airway surfaces of the dog

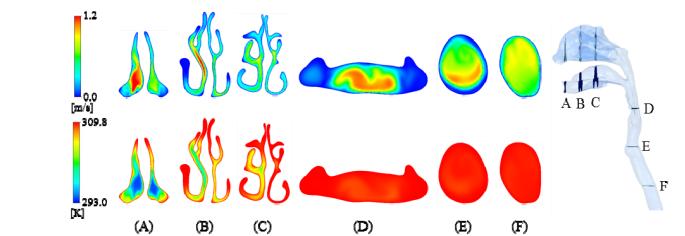
Monkey



(1) $Q_{in}=2.0 \text{ L/min}$ (2) $Q_{in}=4.0 \text{ L/min}$ (3) $Q_{in}=6.0 \text{ L/min}$

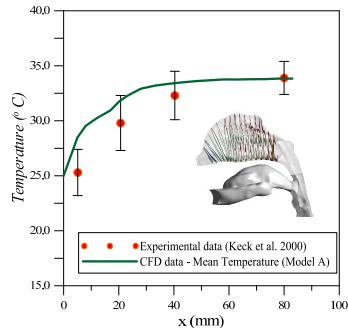
Convective heat transfer flux distributions on the upper airway surfaces of the monkey

Human model (A)

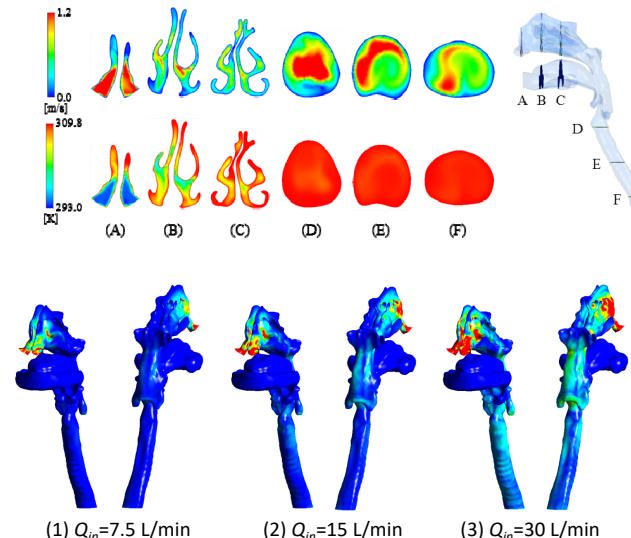


(1) $Q_{in}=7.5 \text{ L/min}$ (2) $Q_{in}=15 \text{ L/min}$ (3) $Q_{in}=30 \text{ L/min}$

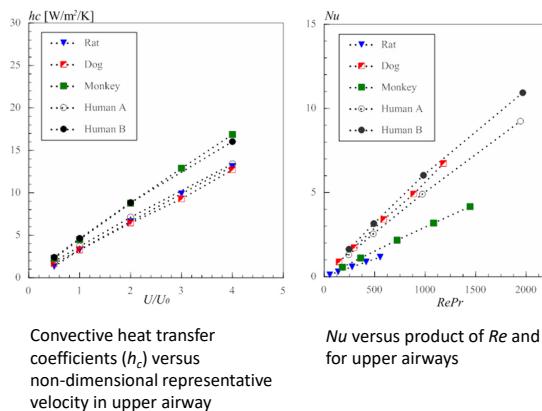
Temperature profiles across the nasal cavity in the case of Model A.



Human model (B)



Nu versus product of Re and Pr for upper airways



$$\begin{aligned} h_c &= \frac{Q_c}{(T_w - T_{air})} \\ Nu &= \frac{h_c D_T}{\lambda} \\ Re &= \frac{u D_T}{\nu} \\ Pr &= \frac{\nu}{\alpha} \end{aligned}$$

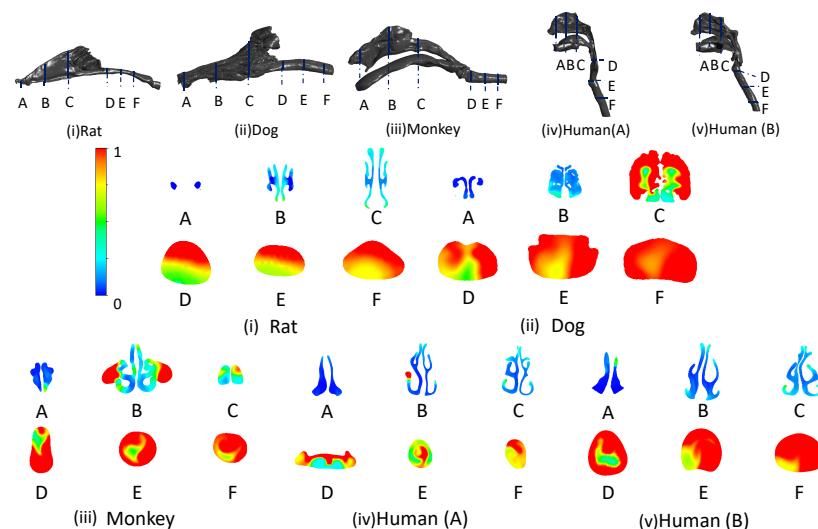
Correlation of Nu versus product of Re and Pr

Target airway model	Correlation function	Range of Re
Rat	$Nu = 0.0021(Re \cdot Pr)^{0.9973}$	$75 < Re < 750$
Dog	$Nu = 0.0069(Re \cdot Pr)^{0.9707}$	$200 < Re < 1600$
Monkey	$Nu = 0.0039(Re \cdot Pr)^{0.9612}$	$250 < Re < 2000$
Human model A	$Nu = 0.0075(Re \cdot Pr)^{0.9414}$	$330 < Re < 2600$
Human model B	$Nu = 0.0107(Re \cdot Pr)^{0.9965}$	$330 < Re < 2600$

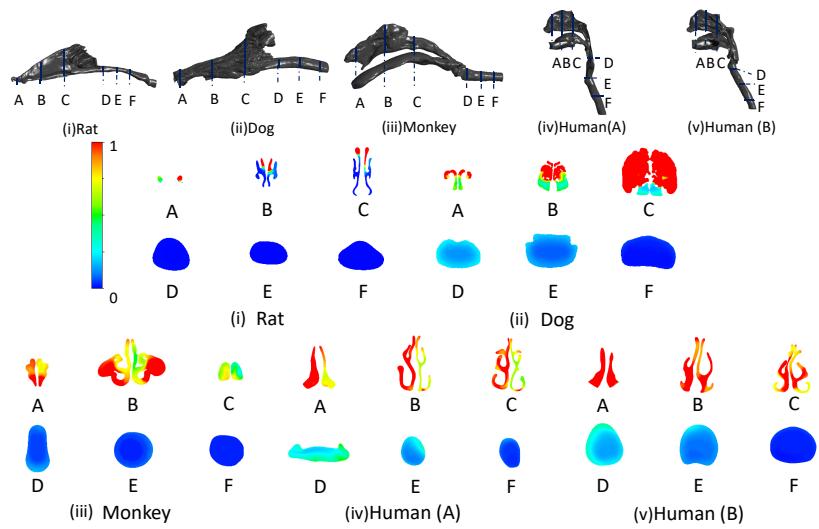
$$Nu = 0.023 (RePr)^{0.854}$$

(Nuckols et al., J Biomech Eng 105(1), 24-30, 1983)

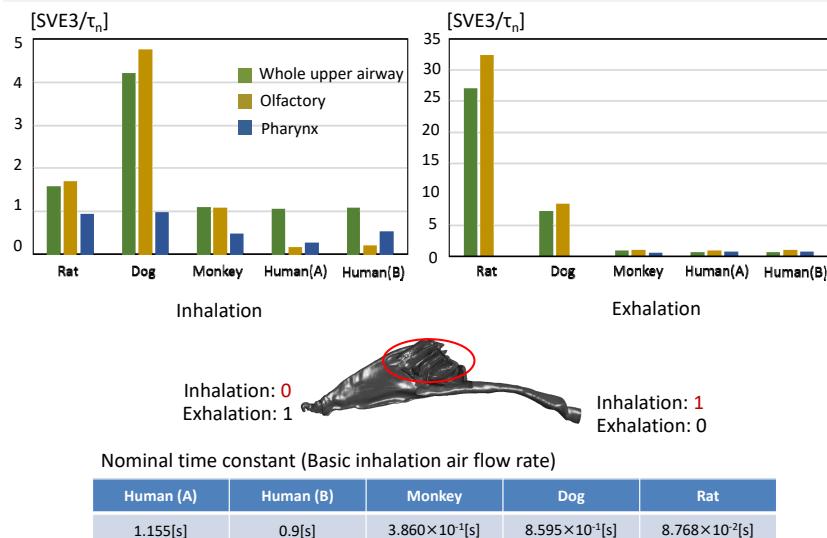
Vent. Efficiency in Respiratory Tracts (Inhalation)



Vent. Efficiency in Respiratory Tracts (Exhalation)



Volume-Averaged Age of Air

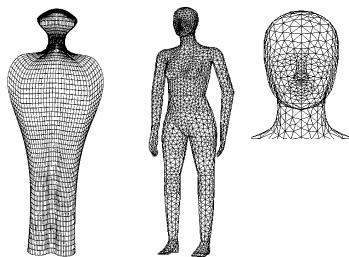


Some arguments for developing *in silico* Human model for Inhalation Exposure Analysis

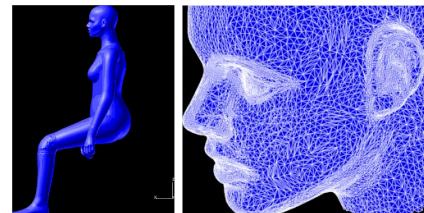


Human Model for CFD

- Micro-Climate analysis around human body
 - Numerical Thermal Manikin, Computer Simulated Person, Virtual Manikin
 - www.cfd-benchmarks.com (Aalborg Univ.)



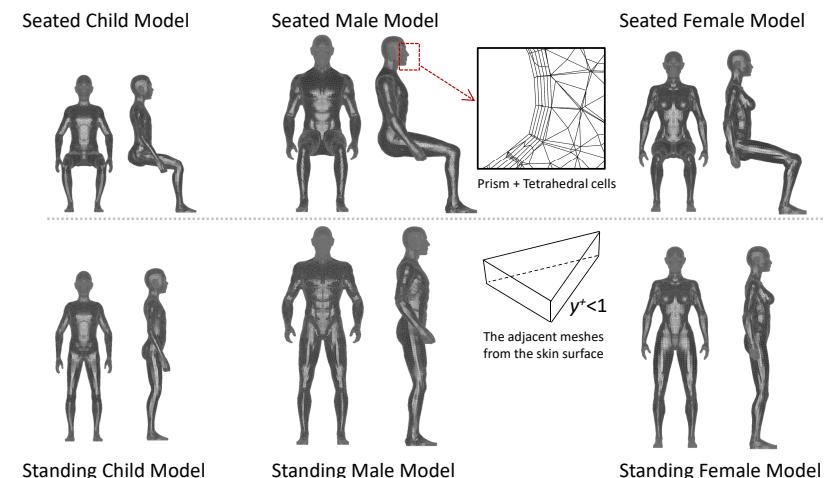
Kato, Murakami (1990)



D. Sorensen (2003)

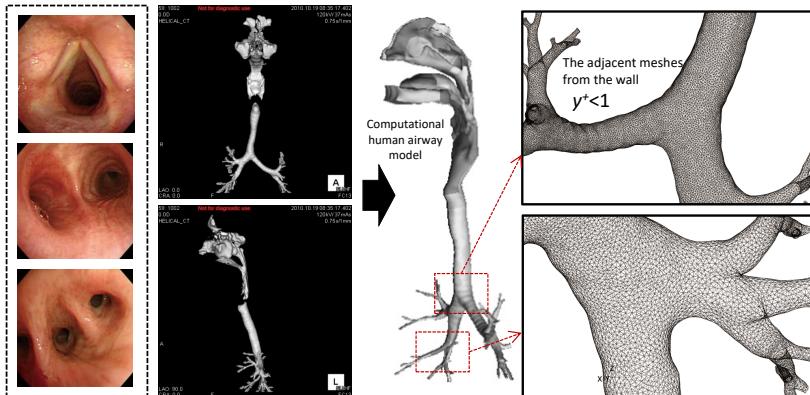
Virtual Manikin

www.phe-kyudai.jp



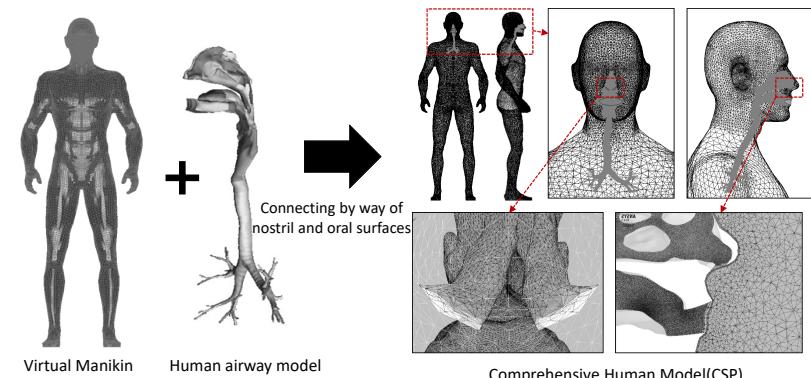
Virtual Airway model for CFD

- From Nasal cavity to Bronchi based on CT data (DICOM format)



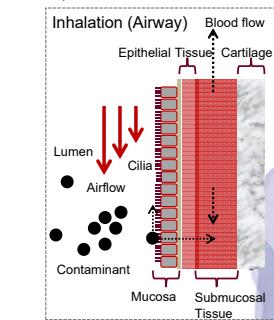
Computer Simulated Person

- Grid design of comprehensive human body incorporating human body geometry and respiratory tract



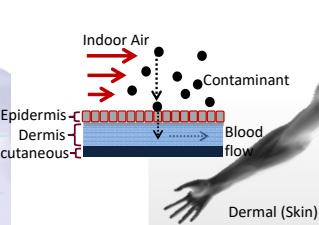
Inhalation and Dermal Exposure Assessment

PBPK for
Inhalation Exposure
Analysis

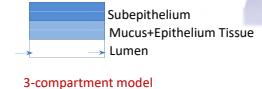


Physiologically Based Pharmacokinetic(PBPK) model

PBPK for
Dermal Exposure
Analysis



Nasal Cavity



$$\frac{\partial C_b}{\partial t} = -K_f \cdot C_b - K_b \cdot C_b - (Q_b/V_b) \cdot C_b + D_b \nabla^2 C_b$$

$$\frac{\partial C_t}{\partial t} = -\frac{(V_{max1C}) \cdot C_t}{K_{m1} + C_t} - K_f \cdot C_t - K_b \cdot C_t + D_t \nabla^2 C_t$$

3-compartment model

Governing Equations of AMTB model

Air

Air flow deposition

$$\frac{d\bar{u}_p}{dt} = \frac{18\mu}{\rho_p d_p^2} \cdot \frac{C_D \cdot Re_p}{24} (\bar{u} - \bar{u}_p) + \frac{(\rho_p - \rho)}{\rho_p} \cdot \bar{g} + \bar{F}_T + \bar{F}_B + \bar{F}_S$$

Lagrangian Discrete Phase Model

$$C_m(y,t)|_{y=0} = \lambda_{ma} C_a(y,t)|_{y=0}$$

Mucosa

Diffusion

$$\frac{\partial C_m(y,t)}{\partial t} = D_m \frac{\partial^2 C_m(y,t)}{\partial y^2} + R_m(C_m)$$

$$-D_m \frac{\partial C_m(y,t)}{\partial y}|_{y=H_m} = -D_T \frac{\partial C_T(y,t)}{\partial t}|_{y=H_m}$$

Tissue

Diffusion

$$C_T(y,t)|_{y=H_m} = \lambda_{Tm} C_m(y,t)|_{y=H_m}$$

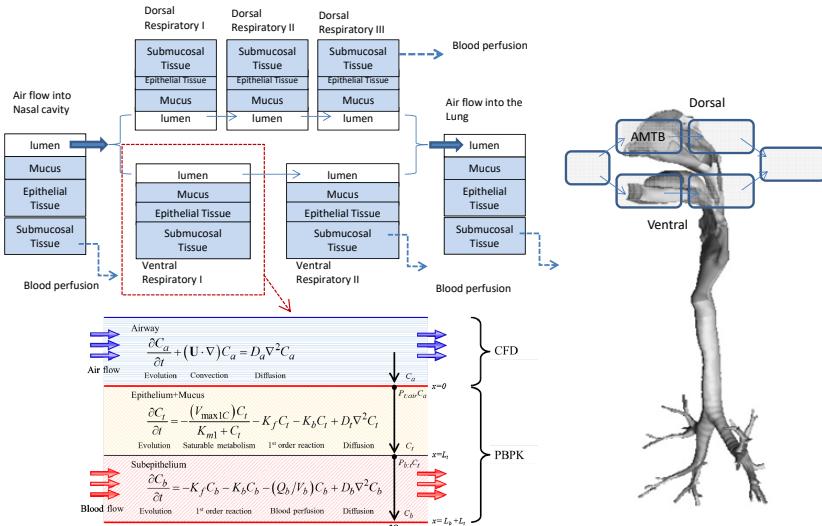
$$\frac{\partial C_T(y,t)}{\partial t} = D_T \frac{\partial^2 C_T(y,t)}{\partial y^2} + R_T(C_T)$$

Blood

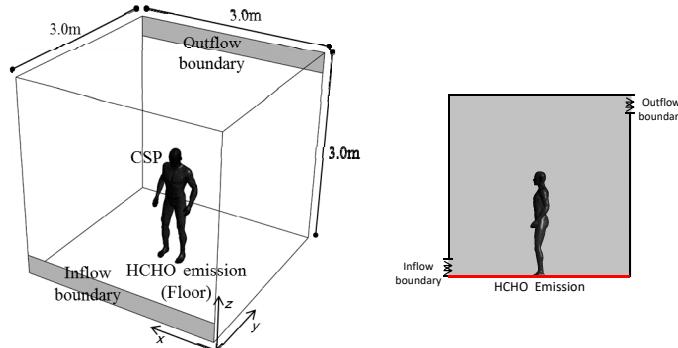
Blood flow

$$C_T(y,t)|_{y=H_m+H_T} = 0$$

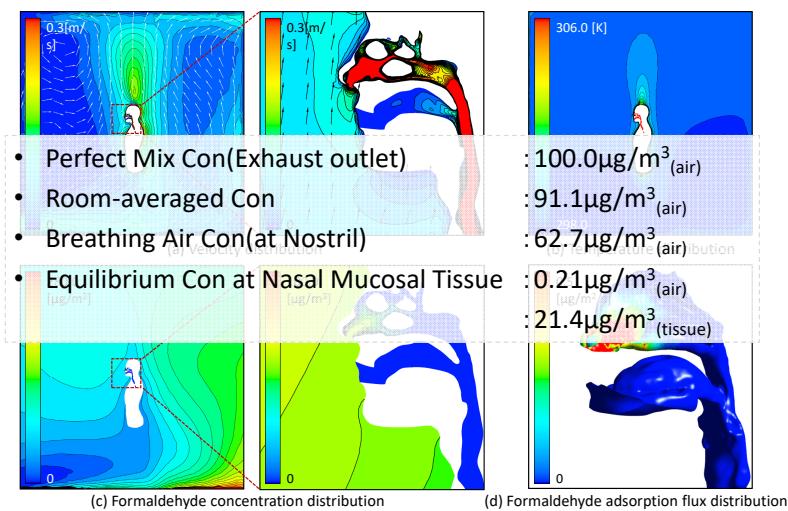
PBPK model (Respiratory Tract)



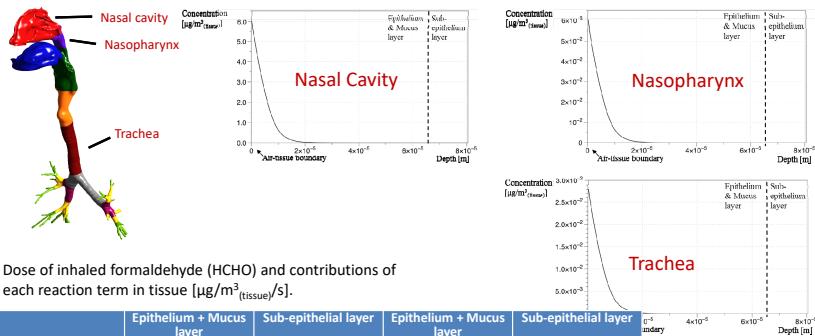
Case Study for Inhalation Exposure (Steady State)



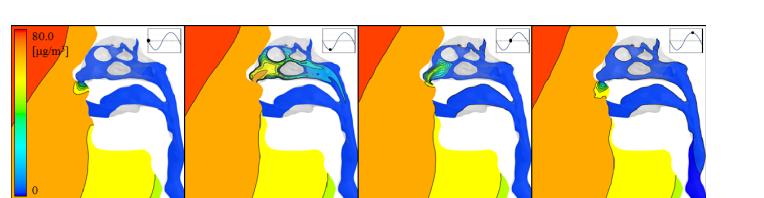
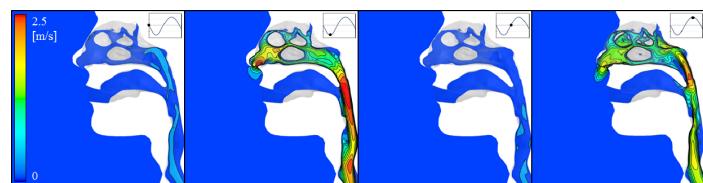
Representative Results



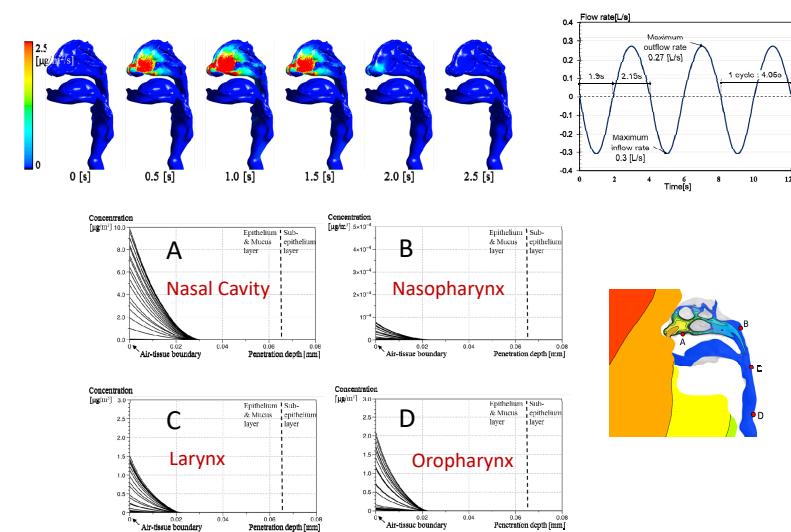
Tissue Dosimetry in Respiratory Tract



Transient Simulation



Time series of HCHO con. profile inside the airway tissue



More detail...

- K Ito*: Toward the development of an *in silico* human model for indoor environmental design, *Proc. Jpn. Acad., Ser. B*, Vol. 92, No.7, 2016, 185-203 (DOI: 10.2183/pjab.92.185)
- NL Phuong, M Yamashita, SJ Yoo, K Ito*: Prediction of convective heat transfer coefficient of human upper and lower airway surfaces in steady and unsteady breathing conditions, *Building and Environ.*, 100, 2016, 172-185
- K Ito*, K Mitsumune, K Kuga, NL Phuong, K Tani, K Inthavong: Prediction of convective heat transfer coefficients for the upper respiratory tracts of rat, dog, monkey, and humans, *Indoor and Built Environ.*, 2016, In press (DOI: 0.1177/1420326X16662111)
- K Ito*: *In silico* human model for fluid-initiated indoor environmental design, Editorial, *Indoor and Built Environ.*, 2017, In press (DOI:10.1177/1420326X17697290)
- K Kuga, K Ito*, SJ Yoo, W Chen, P Wang, Z Liao, J Fowles, D Shusterman, K Kumagai: First- and second-hand smoke exposure assessment from e-cigarettes using integrated numerical analysis of CFD and a computer-simulated person with a respiratory tract model, *Indoor and Built Environ.*, 2017, In press (DOI: 10.1177/1420326X17694476)
- SJ Yoo* and K Ito: Numerical Prediction of Tissue Dosimetry in Respiratory Tract using Computer Simulated Person integrated with physiologically based pharmacokinetic-computational fluid dynamics Hybrid Analysis, *Indoor and Built Environ.*, 2017, In press (DOI: 10.1177/1420326X17694475)